

TITLE OF THE INVENTIONASSEMBLED IMPLANT, INCLUDING MIXED-COMPOSITION SEGMENTCROSS REFERENCE TO RELATED APPLICATION

5 This application is a continuation of U.S. application serial number 09/782,594, filed February 12, 2001, pending, which is a continuation-in-part of provisional application serial number 60/181,622, filed February 10, 2000, and of U.S. application serial number 09/378,527, filed on August 20, 1999, pending, which is a continuation in part of U.S.
10 application serial number 09/191,232, filed on November 13, 1998, pending; and of U.S. application serial number 09/390,194, filed on September 7, 1999, pending; and of U.S. application serial number 29/123,227, filed May 12, 2000, pending, and of U.S. application serial number 09/528,034, filed March 17, 2000, which is a continuation of U.S. application serial number 09/481,319, filed January 11, 2000; and of US Patent
15 application serial number 09/363,909, filed July 28, 1999, and of copending application number 09/905,683, filed September 16, 2001, which is a continuation of copending application number 09/701,933, filed August 25, 1998, which is a continuation in part of 08,920,630, abandoned, filed August 27, 1997; the priority and benefit of which are claimed herein under 35 U.S.C. Sections 119, and 120. All of these applications are
20 incorporated by reference.

FIELD OF THE INVENTION

This invention relates to implants and methods for their preparation wherein components of the implant are assembled from constituent pieces to produce a complete implant. An
25 implant according to this invention comprises two or more segments comprised of mineralized, or demineralized bone segments or a segment comprising both demineralized and mineralized regions juxtaposed to one another.

BACKGROUND OF THE INVENTION

30 In the field of medicine, there has been an increasing need to develop implant materials for correction of biological defects. Particularly in the field of orthopedic medicine, there

has been the need to replace or correct bone, ligament and tendon defects or injuries. As a result, there have emerged a number of synthetic implant materials, including but not limited to metallic implant materials and devices, devices composed in whole or in part from polymeric substances, as well as allograft, autograft, and xenograft implants. It is generally recognized that for implant materials to be acceptable, they must be pathogen-free, and must be biologically acceptable. Generally, it is preferable if the implant materials may be remodeled over time such that autogenous bone replaces the implant materials. This goal is best achieved by utilizing autograft bone from a first site for implantation into a second site. However, use of autograft materials is attended by the significant disadvantage that a second site of morbidity must be created to harvest autograft for implantation into a first diseased or injured site. As a result, allograft and xenograft implants have been given increasing attention in recent years. However, use of such materials has the disadvantage that human allograft materials are frequently low in availability and are high in cost of recovery, treatment and preparation for implantation.

By contrast, while xenograft implant materials, such as bovine bone, may be of ready availability, immunological and disease transmission considerations imply significant constraints on the ready use of such materials.

In view of the foregoing considerations, it remains the case that there has been a long felt need for unlimited supplies of biologically acceptable implant materials for repair of bone and other defects or injuries. This invention provides a significant advance in the art, and largely meets this need, by providing materials and methods for production of essentially any form of implant from component parts to produce assembled implants. In particular, the invention is directed to compositions, methods and kits that relate to an implant, in which at least one single segment is demineralized or comprises a combination of mineralized and demineralized regions. Among the advantages of this invention are the benefits in strength, structural support, and flexibility, depending on the particular implant and its use in a patient in need thereof.

In addition, reference is made herein to US Patent 5,899,939 to Boyce, which issued on May 4, 1999, the disclosure of which is hereby incorporated by reference as if fully set forth herein.

- 5 Finally, reference is made herein to US Patent 6,025,538 to Yaccarino, which issued on February 15, 2000, the disclosure of which is hereby incorporated by reference as if fully set forth herein.

The present invention advances the art beyond the references cited above by disclosing

- 10 and claiming implants that comprise a combination of mineralized and demineralized regions provided in a single segment (discrete piece), which is distinguishable from that disclosed in U.S. Patent No. 6,200,347 (teaching homogenous demineralization of a single segment). The importance of demineralized bone in implants is described in U.S. Patent 6,090,998, and U.S. Patent applications serial numbers 09/417,401, 09/518,000, 15 09/585,772, and 09/778,046, all assigned to the assignee of the present invention, and all of which are incorporated by reference.

SUMMARY OF THE INVENTION

- 20 This invention provides a method for manufacture of autograft, allograft and xenograft implants which comprises assembling such implants from smaller pieces of graft materials to form a larger graft implant product. Some pieces of such graft materials for assembly are demineralized, and are combined with other pieces of graft materials that are mineralized.

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Accordingly, it is one object of this invention to provide a method for assembly of multiple bone implant shapes from smaller bone implant pieces.

- Another object of this invention is to provide assembled bone implants. Related to this
30 object is the object of assembling components of an assembled allograft in such a way as

to compensate for disproportionate shrinkage among components during freeze drying so as to still obtain precision interference fits.

Another object of this invention is to provide a method whereby otherwise wasted tissue
5 may be used in the production of useful orthopedic implants.

Another object of this invention is to provide an implant having a combination of at least one region that is demineralized, juxtaposed to at least one region that is mineralized.

Another object of this invention is to combine a segment of an implant having
10 combination of mineralized and demineralized regions with other segments that are mineralized.

Further objects and advantages of this invention will be appreciated from a review of the complete disclosure and the appended claims.
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BRIEF DESCRIPTION OF THE DRAWINGS

Attached to this invention disclosure are a large number of sketches which demonstrate a wide variety of assembled implants which may be prepared and used according to this
20 invention.

Figure 1 is a flow chart showing the formation of various sub-component parts of an assembled implant according to this invention, from which assembled implants and a kit comprising these parts may be formed according to the disclosure of this invention.

25 **Figure 2** provides a schematic of an assembled implant according to this invention.

Figure 3 provides a schematic of an assembled implant according to this invention.

Figures 4-7 provides a schematic of an assembled implant according to this invention.

Figures 8-9 provides a schematic of an assembled implant according to this invention.

Figures 10-14 provides a schematic of an assembled implant according to this invention.

30 **Figures 15-18** provides a schematic of an assembled implant according to this invention.

Figure 19 provides a schematic of an assembled implant according to this invention.

Figure 20 provides a schematic of an assembled implant according to this invention.

Figure 21 provides a schematic of an assembled implant according to this invention.

Figure 22 provides a schematic of an assembled implant according to this invention.

Figure 23 shows the assembly of a dowel from component pieces.

5 **Figure 24** shows the reinforcement of an implant using a cortical bone pin.

Figure 25 shows the reinforcement of an implant using a cortical bone pin and a cortical bone disc.

Figure 26 shows the reinforcement of cancellous bone implants using a plurality of cortical bone pins.

10 **Figure 27** shows the formation of an assembled implant comprising soft and hard tissues.

Figure 28 shows a segment comprising a central mineralized region and demineralized regions.

Figure 29 shows the arrangement of the segment of Figure 28 positioned between two mineralized implant segments.

15 **Figure 30** shows an alternative embodiment comprising more than one segment having mineralized and demineralized regions.

Figure 31 shows an embodiment of the subject assembled implant supported by a scaffold.

20 **Figure 32** shows an additional embodiment comprising segments fastened together through a friction fit.

Figure 33 shows a two-segment assembled implant fastened together through a friction fit.

Figure 34 shows an embodiment that comprises two segments that interlock together in a transverse cross-over configuration.

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DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

Currently, autograft, allograft and xenograft products are produced as solid, continuous materials. For example, bone dowels (see US Patent 5,814,084, hereby incorporated by

30 reference), Smith-Robinson cervical spine implants, iliac crest grafts, and the like are harvested and machined from single, continuous pieces of bone. The present invention

provides methods for manufacture of autograft, allograft and xenograft implants by assembling such implants from smaller pieces of graft materials to form a larger graft implant product. As a result, increased utilization of valuable implant materials is achieved, thereby more effectively meeting the ever-increasing demands for graft implant

5 materials. In addition, greater flexibility is achieved in the types and shapes of implant materials is achieved. Essentially, any implant piece that may be required may be formed according to the present invention, and orthopedic surgeons may be provided with kits of assemblable parts which may be formed in the course of a surgical procedure to precisely meet the needs of a given patient or procedure. In yet another aspect of this invention,
10 existing graft products may be strengthened or reinforced by assembly of different types of graft materials into an assembled product. One example of such a reinforced product is a cancellous wedge, block, dowel or the like into which is inserted reinforcing pins of cortical bone. As a result, those skilled in the art will understand from this disclosure that different sections of tissue may be assembled to make a complete graft implant.

15 Furthermore, this invention provides for the product of assembled implants comprising any one or combinations of allograft materials, autograft materials, xenograft materials, synthetic materials, metallic materials and the like. Furthermore, the assembled implants or the component pieces which are combined to form the assembled implant may be pre-treated or treated after assembly to incorporate any desired biologically active or inert
20 materials. Thus, for example, in an assembled bone dowel implant according to this invention, the assembled bone dowel comprises segments of cortical bone pinned to each other by means of cortical bone pins. Prior to assembly or after assembly, the graft materials are soaked, infused, impregnated, coated or otherwise treated with bone morphogenetic proteins (BMP's), antibiotics, growth factors, nucleic acids, peptides, and
25 the like.

It is also noted that the compositions and structures disclosed and claimed herein may be obtained from allograft, xenograft or autograft sources, and are comprised of cortical, cancellous, or cortico-cancellous types of bone tissue, or combinations thereof. As
30 disclosed herein, the compositions and structures disclosed and claimed herein are comprised of mineralized bone, demineralized bone, or combinations thereof. Also, a

preferred pre-treatment is to subject allograft and xenograft-sourced bone material to one of the cleansing processes described in US Patent application serial number 09/363,909, filed July 28, 1999, the related PCT application serial number PCT/US00/20629, filed July 28, 2000 and published as WO01/08715A1, and US Patent application serial number 5 09/191,232, filed November 13, 1998.

In essence, one method to reduce antigenicity (disclosed in US 09/363,909 and WO01/08715A1) is to treat bone material in hydrogen peroxide, or hydrogen peroxide in combination with a detergent such as Triton X-100 or Sodium Dodecyl Sulfate (SDS), or 10 another chaotropic agent, such as urea, guanidinium hydrochloride, Tween, TNBP, and mixtures of these agents. This is followed by contacting with a defatting solvent, such as acetone, isopropanol, hexane, or combinations of these. The primary object is to remove the non-collagenous protein from bone graft materials, and thereby reduce antigenicity.

15 In another method, disclosed in US 09/191,232, efficient cleaning and passivation (inactivation of pathogens) is achieved by sequential depressurization and pressurization of a chamber containing bone graft materials, where these materials are being exposed to cleaning/chaotropic solutions and solvents including those described above. This process has been found to improve penetration of the cleaning solutions. Thus, for the bone 20 compositions and structures disclosed and claimed herein, these pre-treatments may be applied to clean and reduce antigenicity of the finished materials.

It will be appreciated that variously shaped wafers, blocks, rings, washer-shaped bone pieces and the like may be affixed to each other in any secure and biologically acceptable 25 manner. Preferably, the assembled pieces of bone are affixed to each other by means of pins, screws, rods, interference fit, threaded fits, key-way fit, and the like made from cortical bone. These fixation pieces are machined in a CNC lathe or the like to appropriate dimensions and are then threaded into mating holes tapped in the pieces to be assembled, or are pressed into drilled holes through adjacent pieces to be assembled by a 30 pneumatic press or the like. In this fashion, very strong and tightly fitted pieces of implant materials may be joined and implanted. The assembled pieces may first be

machined to desired dimensions and shapes, prior to assembly, the assembled implant may be machined, or both.

As noted above, the implant according to this invention may comprise an assembled cancellous block, dowel or the like, harvested from the iliac crest or another suitable site. As is known in the art, due to the wafer-like structure of cancellous bone, such grafts have low load-bearing characteristics. There exist reports in the literature of instances of extrusion, expulsion or collapse of iliac crest wedges, Cloward Dowels, and the like when utilized, for example, in spinal fusions. Nonetheless, use of cancellous bone is preferable over use of cortical bone implants, since cancellous bone is more osteoconductive than cortical bone. According to this invention, a Cloward Dowel, iliac crest wedge, or cancellous bone block, dowel or the like is reinforced by insertion therein of cortical bone pins. According to the method of this invention, cortical implants may also be reinforced by insertion therein of cortical bone pins, including when an assembled implant is prepared comprising different segments of cortical bone, cancellous bone or both. Insertion of the reinforcing pins provides an implant with multiple load-bearing pillars. The pins may be made to protrude from the surface of the implant to engage with inferior, superior or both surfaces of bone between which the implant is inserted. Thus, in a spinal implant, pin protrusions may be employed to create contact between the implant and the vertebral bodies, thus preventing extrusion and reinforcing a secure fit of the implant between adjacent vertebrae. We have, surprisingly, found that cortical pins of about 4.5 mm in diameter may each support a load of up about 2700 newtons (160 Mpa). Thus, according to the method of this invention, multiple pins may be inserted into an implant to produce a load-bearing capacity of known proportions (e.g. 10,000 newtons by insertion of five pins).

A further advantage of this invention is that it permits use of tissues that are not currently amenable to standard autograft, allograft or xenograft harvesting and processing procedures, such as ribs, metatarsal bone and the like. In addition, useful implant materials may be harvested and produced from otherwise un-useable donor tissues. In addition, due to the different nature of various segments of bone that are incorporated

into the assembled, reinforced implants of this invention, various shaping methods aside from CNC lathe or other known procedures may be applied to different segments of the implant. Thus, a cancellous portion of bone implant may be compression molded, and then affixed to other portions of cortical or cancellous bone machined according to
5 different or similar principles. In addition, due to the ability provided by this invention to assemble implant pieces, implants of unusual sizes and dimensions may be prepared and machined. Thus, implants of 100 mm in size could be machined, for example, for corpectomies, when otherwise bone stock for manufacture of such implant dimensions would not be available.

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In view of the present disclosure, it will be appreciated that this invention provides a wide variety of assembled implants and implant parts: dowel shaped implants comprising assembled dowel segments, between about two to about ten segments, pinned together by one or more cortical bone pins. The assembled segments may closely abut each other or
15 may be spread apart from each other. Such implants may be prepared by harvesting discs of cortical bone, drilling and optionally tapping holes therein, and inserting shafts of cortical pins therethrough, or therein, optionally by threading portions thereof for torquing into optionally tapped holes. The thus produced dowels may be tapered or have parallel sides. In addition, dowels which are harvested as a cross-section across the
20 intramedullary canal of a long bone, as in US Patent 5, 814,084, which might otherwise not pass production specifications, due to penetration of one outside wall into the intramedullary canal, may be completed by insertion therein of a cortical pin. Likewise, where a sidewall is otherwise considered to be too narrow, a “doughnut” of bone may be affixed to the sidewall by means of a cortical pin. A longer dowel may be prepared by
25 affixing two dowels to each other. A posterior longitudinal interbody fusion implant (PLIF) may be machined from a single piece of cortical bone, or be assembled from two pieces of bone which are affixed to each other by means of a cortical pin. A bone screw may also be prepared according to the method of this invention by affixing multiple pieces of cortical bone to each other with a cortical bone pin, and then machining a thread
30 on the exterior of the assembled bone pieces. It will further be appreciated from this disclosure that different portions of the assembled implant may be demineralized,

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partially or fully, to achieve a level of elasticity or compressibility not otherwise present in cortical or cancellous bone. Specific embodiments of assembled implants having a combination of demineralized and mineralized regions, present or assembled into a single discrete piece (i.e., a segment), are shown to possess superior properties. Different 5 portions of bone may also be retained on a shaft by means of a cotter-pin type device.

According to one embodiment, a segment is mineralized allograft bone, and this region may be intimately contacted on two sides by two regions of partially demineralized allograft bone. Demineralized regions of a single segment may be formed according to

10 conventional methods, such as by dipping a portion of a segment of mineralized allograft bone in a demineralizing acidic solution to demineralize that portion while leaving the adjacent portion mineralized. Alternately, a segment of a larger assembled implant comprising both mineralized and demineralized regions may be formed and later joined together (such as by biocompatible adhesives, bone pastes, tongue and groove, etc.) into a structure that is or can be divided (such as cut transversely) into a number of segments 15 and subsequently assembled. The term “demineralized” is well known in the art, and for the purposes of this invention is defined to be the removal of minerals, such as by dissolution in acid, from a material such as bone.

20 As used herein, a “mixed-composition segment” is defined to describe a segment of an allograft implant that is comprised of two or more regions having different characteristics and/or properties. For example, a mixed-composition segment can comprise a region comprising demineralized bone or mineralized bone attached to another region comprising a synthetic material. Also, it is noted that “demineralized,” when not 25 preceded by either “partially” or “fully,” is taken to include, subject to the specific context, both partially and fully demineralized. Also, when referring to a particular mixed-composition segment, the segment may be described as a “demineralized bone segment comprising a region of mineralized bone,” and this is taken to mean a segment that has at least one region of mineralized bone and at least one region of demineralized 30 bone.

In addition to assembled implants, instruments may be conveniently prepared according to the methods of this invention which may be utilized for insertion of other implants. In one embodiment of this invention, therefore, an implant driver is produced wherein the driving mechanism itself is formed from assembled cortical pins which protrude into 5 mating recesses in an implant device. The instrument may be torqued to adequate loads to induce implantation of spinal implants and the like.

In developing the various embodiments of the present invention, one technical issue of merit is the need to develop a process whereby donor tissue, whether hard or soft tissue, 10 allograft or xenograft tissue, may be treated in such a fashion as to eliminate the possibility of cross contamination between tissue segments obtained from different sources. While it is possible to practice the present invention to advantage using tissue obtained from a single screened donor, the real economies of scale and commercially viable application of the present technology is best realized by implementation of an 15 efficient and reliable tissue decontamination process. Ideally, the process is one which permits multiple segments of soft or hard tissue to be treated simultaneously so that a stock of materials for assemblage of implants according to the present invention is facilitated. Accordingly, on preferred method for treatment of tissue, disclosed in PCT publication WO 00/29037, the disclosure of which is hereby incorporated herein by 20 reference as if fully set forth herein (and priority of the US Patent filings which gave rise to this application is hereby claimed for that purpose). Accordingly, in this aspect of the invention, a process is claimed whereby an assembled allograft or xenograft tissue implant is prepared by treating the tissue in a closed container in which different cleaning solutions are contacted with the implant segments, either before or after assembly and 25 machining into the final implant form, either in the presence or absence of sonication, with rapid oscillation of pressure in the closed container, to achieve deep cleaning and interpenetration of cleaning solvents into the interstices of porous implants or tissues. Solutions including, but not limited to detergent solutions, peroxide solutions and the like are used in such procedure, and terminal sterilization with gamma irradiation, gaseous 30 sterilants known in the art or other terminal sterilization procedures known in the art are

employed to ensure safe implantation of the assembled implants according to this invention.

Referring now to figure 1, there is shown a flow-chart representing various elements that may be processed and assembled according to this invention. Cortical bone pins 100 are used to assemble a series of bone discs 101 into a pre-part 102 which is then machined into a series of final products: Threaded dowels, 103; small blocks 104; unique shapes, 105 such as a “wedding-cake” like shape wherein discs bearing threads are spaced apart from each other leaving voids 105' into which additional materials may be inserted, with the discs retained in fixed relation to each other by means of the through pins 100; tapered dowels 106; screws 107; smooth cylinders 108; or large blocks 109. From this figure, it will be appreciated that a central concept relevant to the present invention is the ability to machine smaller parts of tissue, specifically bone tissue, such as cortical bone, cancellous bone, cortical-cancellous bone, portions of which may be demineralized (see, for example, US Patent 6,090,998, hereby incorporated herein by reference for this purpose), and assemble these portions of tissue using, preferably, cortical bone pins. The assembled tissue pieces may be machined prior to assembly, and then, upon assembly, a complete implant is ready for implantation. Alternatively, the tissue pieces may first be assembled, and the assembled pieces may then be machined into any desired final form. The order of assembly and machining will be determined by the specific forms of implant required for a particular application. In figure 1, a series of pre-machined tissue forms are disclosed, which may conveniently be included in a kit for use as needed by an orthopedic surgeon. Thus, for example, where a particular implant of specific dimensions is required, the surgeon is able to select pre-shaped implant segments to fill a particular geometric space and shape in the spine of an implant recipient. Numerous permutations and combinations of implant pieces for assembly are possible, based on the pre-machined assemblable implant pieces included in such a kit, and those skilled in the art will appreciate that the skilled orthopedic surgeon will be able to create implants as needed when supplied with such a kit. Thus, a preferred kit includes discs of bone, cortical bone, cancellous bone, allograft or xenograft, also referred to herein as “washers” or “doughnuts” such that a center hole is provided for press-fitting or screwing on of the

discs to a cortical bone or synthetic or metallic shaft or pin. The discs may be demineralized, mineralized, or partially demineralized. Also desirable in such a kit are plugs of cortical bone, cancellous bone, or cortical-cancellous bone, including at least one through hole, and optionally more than one such through hole, for insertion of pins

- 5 therethrough. Ovals, squares, rectangles and irregular shapes may also be provided in certain kits for specific applications. It will further be appreciated, based on the present disclosure, that inclusion of a bone paste, such as that disclosed in WO99/38543, hereby incorporated by reference, may be beneficial for filling any voids that remain, and to implant with the assembled implant, osteogenic material, (i.e. osteoconductive material,
- 10 Osteoinductive material, or both, as well as material that assists in adhering the implant to the site of implantation). Further, a molded implant may be combined with the assembled implant of this invention. A preferred molded implant for orthopedic applications is disclosed in PCT publication WO 00/54821, the disclosure of which is hereby incorporated by reference.

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- It is noted that assembled allografts may be assembled at and distributed from a central location, or, as discussed above, assembled around the time of surgery to meet a specific requirement of a patient in need thereof. In many applications it is desirable to have a tight and accurate interference fit between cortical bone pins and the holes in bone pieces that are connected by the bone pin. The target range for such an interference fit is 0.001 to 0.003 inches (e.g., the pin diameter is 0.001 to 0.003 inches larger than the hole diameter, and is pressed fit into place). However, it has been learned that freeze-drying the pins and other bone pieces exerts a disproportionate shrinkage upon the pins compared to the hole diameters. That is, the pin shrinks slightly more than the hole.
- 20 Uncorrected, this would result in a less accurate, and less acceptable, interference fit.

- 25 The following method has been adopted to solve this problem. A bone pin, preferably of cortical bone, of a desired diameter is vacuum dried for at least five hours. This drying is preferably at room temperature and at a negative pressure of approximately 100 milliTorr. This pre-treatment results in a shrinkage of approximately 80 percent of the total shrinkage that would occur in freeze drying. The pin diameter is measured, and a

hole is made in the discs (or other shapes that are to be assembled) using an appropriately sized reamer. The target size for the hole is 0.002 to 0.0025 inches smaller than the post-vacuum drying pin diameter. Preferably, prior to this drilling the discs or other shapes have been kept saturated with moisture to maintain a consistent size and subsequent

5 shrinkage percent. After all holes are drilled, the pin(s) and discs or other shapes are assembled, and then freeze dried. The resulting assembled allografts have been found to have interference fits in the desired target range. This method is applicable to the various embodiments described in this disclosure. Alternatively, where segments are provided in a kit for assembly prior to surgery, the discs and pins are preferably freeze-dried as
10 disassembled. After freeze-drying, the diameter of the pins is measured and the appropriate size hole is made in the disc. This allows the provision of multiple parts in a kit, wherein the parts can be assembled together such that the requisite friction is achieved to keep the parts securely together.

15 With reference to figure 2, there is shown two machined bone pieces, **T** and **Z** each of which bear external threading **X** and holes **Y** into which pins **A** are inserted to form the assembled graft **200**. As can be seen, the assembled graft **200** comprises a void, **201** into which osteogenic material may be inserted prior to or after implantation. The pins **Y** may be metal pins, but preferably are pins machined from cortical bone. This enables the
20 entire implant to remodel into autogenous tissue over time, such as vertebral bone, when the implant **200** is inserted into the intervertebral space. The graft **201** is also shown with a groove, **202** in which a driver may be inserted to provide rotational torque for insertion of the implant. An instrument attachment hole, **203**, is also provided, to ensure that the implant remains securely on the head of the driver means in the process of surgical
25 implantation. Naturally, those skilled in the art will appreciate that the segments **Z** and **T** may be brought into close abutment with each other, thereby eliminating the space **201**. In that event, the length of the pins **A** would be modified to prevent unnecessary protrusion, although in some applications, protrusion may be useful when driving the implant **200** into place. It will also be appreciated that the number of pins used, while
30 represented as two in this figure, may be fewer or more in number, depending on the particular application, the extent of torsional or compressive loads, and the like

anticipated to be experienced by the implant once *in situ*. In some applications, the insertion of reinforcing cortical bone pins establishes a pillar structure such that two or more cortical bone pins are load-bearing. This application allows the use of materials in the segments that do not initially bear a substantial load, that load being born by the 5 cortical bone pin pillars, and these materials have the opportunity to reform into bone that will provide subsequent structural load-bearing.

Figure 3 shows an implant assembled from three principal segments **F**, **D**, and **E**, which are held together by pins **300**. In this implant, the waffle-shaped structure of implant 10 segment **D** is intended to represent the use of cancellous bone, which is abutted on either side by cortical bone, which forms segments **F** and **E**. The fully assembled implant is shown in figure 4, while figures 5, 6 and 7 show end-on views, and cross sectional views A-A and B-B, respectively. Those skilled in the art will appreciate from this disclosure that segment **F**, segment **D**, or segment **E** may be demineralized according to methods 15 known in the art. Likewise, all of these segments may be demineralized. Where a flexible implant is required, the implant may be assembled, and the entire implant may be demineralized. Where flexibility is important in one dimension and structural support is also required, one solution is to have one or more segments of an composite bone graft be a mixed-composition segment which comprises at least one mineralized region and at 20 least one demineralized region (described in detail below).

Figure 8 shows an embodiment of this invention wherein rectangular bone segments **N** and **G** are assembled into implant **900**, shown in figure 9. Features **901** and **902** which comprises ridges, teeth, or other external features are machined into the superior and 25 inferior faces of the implants in order to assist in retention of the implants once placed *in situ*.

Figures 10-14 show the assembly of elements **J**, **H**, and **I** into implant **1100**, shown end-on, in cross-section A-A and B-B, in figures 12-14, respectively. As can be seen, bone 30 element **H** is shown with a waffle-like structure, to represent that this element may be cancellous bone, demineralized bone, a polymer composite, such as poly-L-Lactic acid,

polyglycolic acid, or the like. Features **1101** and **1102** represent external grooves or teeth machined into the superior and inferior surfaces of the implant to assist in retention of the implant once placed *in situ*.

- 5 Figures 15-18 show the assembly of elements **M**, **K**, and **L**, each of which is a substantially cubic bone element, using pins **1500**. Figure 17 is a top view, showing cross section A-A, represented in figure 18, with the final assembled implant **1600** shown in figure 16.
- 10 Figure 19 shows a “Wedding-Cake” design of an implant **1900** assembled from units **A-C**, pinned together by pins **a-c**. Void area **1901** is available for filling with osteogenic materials.
- 15 Figure 20 shows implant **2000** which is an assembled Cervical Smith Robinson implant similar to that shown in PCT publication WO99/09914, hereby incorporated by reference. This implant is fashioned from a series of assembled bone pieces **2001** and machined into the desired final shape.
- 20 Figure 21 shows implant **2100** assembled from two cortical bone pieces and one cancellous bone piece, and pinned together. The implant has an anterior height **H1** which is smaller than posterior height **H2**, which permits retention of correct spinal lordosis upon implantation, for example, in a posterior lumbar intervertebral implant fixation procedure. Superior and inferior features **2101**, **2102** prevent expulsion of the implant once place *in situ*.
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- Figure 22 shows an implant **2200** assembled from a series of sub-implant pieces **2201**. The implant may contain cancellous bone **2202** segments, as well as cortical bone **2203** segments and cortical bone pins **2204**.
- 30 Figure 23 shows the formation of a tapered dowel **2300** by assembling “doughnut” or “disc” or “washer” shaped bone pieces **2301** on a cortical bone shaft **2302** by using

washer pieces of differing diameter. This figure only shows two discs, but a continuous dowel is formed by using discs of a graded diameter between each end of the cortical bone shaft **2302**. In figure 24, figure 24A shows a bone dowel in which one sidewall of a bone dowel **2400** such as that disclosed and claimed in US Patent 5,814,084, hereby incorporated by reference, is “out of specifications” due to being too narrow or absent. This is repaired in figure 24B according to this embodiment of the invention by incorporation of an allograft or xenograft cortical bone pin **2401**, to form a complete bone dowel. In this manner, valuable biological material which might otherwise be unusable for a particular application may be salvaged for use by employing the methodology of this invention.

In figure 25, a similar procedure for salvaging a dowel **2500** is shown whereby a pin **2501** is driven through the center of the dowel **2500** to reinforce the dowel longitudinally. Furthermore, where an endcap **2503** of the dowel is “out of spec” for being too narrow, the endcap is reinforced by press-fitting a cortical bone disc **2502** onto the end of the pin **2501**.

In figure 26, a series of cancellous bone implants **2600** are reinforced by inclusion therein of a series of cortical pins **100**. Each cortical pin of a 2 mm diameter has been found to support approximately 2000 newtons of axial compressive load. Accordingly, cancellous bone implants of essentially any desired height and compressive strength may be assembled in this manner by affixing several layers of cancellous bone with cortical bone pins. Naturally, based on this disclosure, those skilled in the art will appreciate that other materials may be included in such a “sandwich” of bone materials. The cancellous bone may be soaked in a solution containing growth factors, such as, but not limited to, bone morphogenetic proteins, fibroblast growth factors, platelet derived growth factor, cartilage derived morphogenetic proteins, stem cells, such as mesenchymal stem cells, osteoprogenitor cells, antibiotics, antiinflammatory compounds, anti-neoplastic compounds, nucleic acids, peptides, and the like. Those skilled in the art will also appreciate that layers of cortical bone may be included, layers of biocompatible synthetic polymers and the like may also be included in the stacked bone implant. Various shapes

may also be built upon, using for example, circles, ellipses, squares, and the like, as necessary for a given application.

In a further aspect of the present invention, the assembled implant is driven by cortical pins to seat in an implant site, using a driver that engages cortical bone pins with purchase sites on the implant. Thus, for example, not meant to be limiting, the driver may comprise a handle with projecting cortical pins which engage with holes in the assembled allograft, thereby providing a site for torquing the implant into position.

- 10 In a further embodiment according to this invention, assembled cortical bone blocks, or cortical cancellous bone blocks, or bone blocks comprised of a combination of cortical bone, cortico-cancellous bone, cancellous bone, and/or synthetic materials as described elsewhere herein, are assembled in combination with wedged or pinned soft tissue, such as tendon, ligament, skin, collagen sheets, or the like, to create grafts similar to naturally occurring tissue sites, such as the bone-tendon interface found at the patella. Such combination implants permit reconstruction of sites such as the Anterior Cruciate Ligament (ACL) or Posterior Cruciate Ligament (PCL). According to one embodiment of the invention, a ligament or tendon or skin or collagen sheet membrane is pinned between adjacent blocks of cortical bone. Accordingly, various implants, such as known bone-tendon-bone implants which are in short supply may be supplanted by assemblage of an implant comprising assembled bone blocks, between which is fixed a ligamentous tissue, including but not limited to ligament, tendon, demineralized bone, and the like.
- 15 Referring to figure 27, there is shown one example of this embodiment of the present invention in which an implant 2700 is assembled from a superior bone block 2701, an inferior bone block 2702 and a wedged flexible tissue, such as a ligament or tendon or portion of demineralized bone 2704, all of which are pinned together with cortical bone pins 2703 or other fixation means. The superior bone block, 2701, is comprised of three segments of bone, 2701a-c, pinned together by pin 2715. Naturally, those skilled in the art will appreciate, based on this disclosure, that other shapes of bone blocks, such as rounded bone blocks, and other types of combinations of soft and hard tissues may be assembled according to this disclosure. However, the example of such an implant 2700

may be used instead of having to harvest a bone-tendon-bone implant from cadaveric knees, which tissue is in short supply.

Another variation of this embodiment is to construct a bone-tendon-bone type of implant
5 that is comprised of at least one block made from substantially synthetic materials,
attached to a tendon-like section of an allograft, autograft or xenograft sourced ligament,
tendon, skin or collagen. Still another variation is to construct a bone-tendon-bone type
of implant that is comprised of a synthetic tendon-like material, attached to a block at one
or both ends, where the block is comprised of allograft, autograft or xenograft bone, and
10 the block is a single piece or a multi-segment assembled bone graft. Examples of
synthetic materials, not meant to be limiting, are biocompatible materials selected from
the group consisting of nylon, polycarbonate, polypropylene, polyacetal, polyethylene
oxide and its copolymers, polyvinylpyrrolidone, polyacrylates, polyesters, polysulfone,
polylactide, poly(L-lactide) (PLLA), poly(D,L-lactide) (PLA), poly(glycolide) (PGA),
15 poly(L-lactide-co-D,L-Lactide) (PLLA/PLA), poly(L-lactide-co-glycolide) (PLA/PGA),
poly(glycolide-co-trimethylene carbonate) (PGA/PTMC), polydioxanone (PDS),
polycaprolactone (PCL), polyhydroxybutyrate (PHBT), poly(phosphazenes), poly(D,L-
lactide-co-caprolactone) (PLA/PCL), poly(glycolide-co-caprolactone) (PGA/PCL),
poly(phosphate ester), polyanhydrides, polyvinyl alcohol, and hydrophilic polyurethanes.
20 These materials, some of which are bioabsorbable, can be used in combination with one
another to form the synthetic section of the graft.

Another aspect of the invention is an allograft segment wherein at least one region is
mineralized, and at least one region is demineralized. For example, Figure 28 depicts an
25 allograft unit, 2800, that has a central mineralized region, 2801, with two demineralized
regions, 2802 and 2803, one to either side of the mineralized region. Two holes, 2804,
pass from the top, 2805, to the bottom, 2806, of the allograft segment, 2800. As
described above, these holes, 2804, are used for assembly of this segment with other
segments, as by passing pins, dowels, or other attachment means through the holes to
30 connect two or more allograft segments in a line.

One method of producing this segment is to start with a fully mineralized piece of allograft of the shape depicted in Figure 28. One side, such as that represented in Figure 28 as **2802**, is subjected to an appropriate acid demineralizing regime (such as described earlier in this application) until it is to a desired level of demineralization for the purpose 5 of the allograft segment, **2800**. Then the opposing side, **2803**, is similarly subjected to said regime. The regions exposed to the demineralizing regime are immersed in suitable solutions to remove acids and other components that may be toxic, inflammatory, or inhibitive of cellular infiltration. The middle mineralized region does not contact the acid solution of the regime. The resultant segment is referred to as a mixed-composition 10 segment (“MCS”). As described below, this may be combined with other segments to form an assembled allograft.

The demineralizing regime is varied depending on the desired results. In one example, a central demineralized area is produced by blocking the outside surfaces (sides and top 15 and bottom surfaces near the sides) of a cylinder of bone, allowing acid solution exposure only to a central circular area. In this and in other exposure regimes, a transition zone of demineralization may exist between the target area (subject to demineralization) and the blocked area (designed to remain mineralized), in which the degree of mineralization changes from the exposed demineralized region to the non-exposed mineralized region. 20 The extent of the transition zone can vary, and can be adjusted to some extent by the demineralization regime to better meet a particular application for the implant.

An alternative means of producing an allograft segment such as **2800** is to prepare one or more demineralized regions and assemble them with one or more mineralized regions. 25 The assembly would be secured together by means previously described. This is referred to as an assembled mixed-composition segment (“AMCS”), which may be further combined with other segments to form a larger assembled allograft.

It is noted that the degree of demineralization spans a broad range, with increased 30 exposure to acid (whether by time, acidity or solution, frequency of change-out of solutions, or any combination) resulting in a more demineralized, more flexible material.

Thus, an implant or implant region may be partially demineralized, wherein some minerals remain and there is a range of flexibility. Alternately, an implant or implant region may be fully demineralized, wherein the minerals are basically removed and there is a maximum flexibility. As noted, during the demineralization of one region of a MCS,
5 a transition zone may occur between the region being demineralized and an adjacent region of mineralized bone material.

Thus, an allograft segment, whether formed by either of the means described above for Figure 28, may be comprised of one or more fully mineralized regions in combination
10 with one or more partially demineralized regions, or with one or more fully demineralized regions, or with a combination of partially and fully demineralized regions. The arrangement in Figure 28 is not meant to be limiting, but merely illustrative of the concept of forming or assembling two or more regions or two or more types of
15 allografts (mineralized, partially demineralized, fully demineralized) into a single allograft segment. Thus, a wide variety of geometric arrangements may be made or assembled.

An allograft segment as described above can be combined with other allograft segments as exemplified in Figure 29. Figure 29 shows a first segment, **2901**, that is fully
20 mineralized, and a second segment, **2903**, that is also fully mineralized. Positioned between these segments is a mixed allograft segment, **2902**, such as described above in Figure 28. Two pins, **2904**, are used to secure the three segments together. Once assembled, this allograft assembly can be used in a patient in need of a degree of flexibility in the A-A dimension. Such flexibility is provided largely by the flexibility of
25 the partially or fully demineralized side regions of the mixed-composition allograft segment, **2904**. Additional flexibility may be provided by the flexibility of the pins, **2904**, and the spacing between the segments, **2905**.

This flexibility is advantageous post-operatively by reducing potential areas of high
30 compression between an allograft implant and adjacent autologous bone structures. Another potential advantage for certain procedures and implants, the region(s) of

demineralized or partially demineralized may remodel more rapidly and/or more strongly than the region(s) of mineralized bone. The mineralized bone region(s), however, provide structural support to transfer load during the remodeling of the demineralized or partially demineralized region(s).

5

Also, as described in U.S. patent 6,090,998 and its daughter applications, demineralized or partially demineralized areas of an implant may provide flexibility that is used to simulate joint flexibility.

- 10 It is further noted that the present invention provides for fabrication of implants having specific, even complex, patterns of flexibility or “shock-absorbing” characteristics based on the use of MCS and/or AMCS positioned at specific orientations to other segments of an assembled allograft and to the structure in the patient in whom the implant is implanted. One example of this is depicted in Figure 30. An assembled allograft, 3000, 15 comprises two MCS, 3001 and 3002, which are oriented approximately 60 (and approximately 120, from a second aspect) degrees apart in relation to one another. The first MCS, 3001, permits shock absorption in the plane defined by A-A, and the second MCS, 3002, permits shock absorption in the plane defined by B-B. This allows for complex shock absorption/flexibility patterns. MCSs 3001 and 3002 are attached by a single pin connector (not shown) passing through hole 3003. The assembled allograft 20 may include additional segments that are not MCS or AMCS, in combination with MCS or AMCS. Variations in design and construction will result from the specific requirements for an implant and the particular skill in the art as to a design or assembly means. Such variations are within the scope of the invention disclosed and claimed 25 herein.

Regarding the assembly of an AMCS, one line of construction is to surround and/or support the separately prepared regions that are assembled together to form a segment with synthetic scaffolding. For instance, three regions, two demineralized with one 30 mineralized region between (such as in Figure 28) may additionally comprise a processed collagen sheet that is rolled around the assembled three regions. Also, rigid or semi-rigid

synthetic structures may be used as noted above. The supplemental materials are to provide additional strength and lessen the bonding strength required on the surfaces between regions of the AMCS.

- 5 Another aspect of the invention is the use of synthetic segments and/or scaffolding in conjunction with an assembled allograft, where the assembled allograft is comprised of any combination of one or more segments each of: mineralized bone; partially demineralized bone; fully demineralized bone; or MCS or AMCS of these materials. One or more segments of assembled implants as described herein may be substituted by a
- 10 synthetic segment. In addition, synthetic materials can be in the form of various scaffolding used in conjunction with one or more of the assembled segments. The synthetic segment or scaffolding may be comprised of various materials, including, but not limited to stainless steel, titanium, cobalt chromium-molybdenum alloy, and a plastic of one or more members selected from the group consisting of nylon, polycarbonate,
- 15 polypropylene, polyacetal, polyethylene oxide and its copolymers, polyvinylpyrrolidone, polyacrylates, polyesters, polysulfone, polylactide, and a combination of one or more bioabsorbable polymers.

In particular, biodegradable polymers suitable for use in the present invention include:

- 20 poly(L-lactide) (PLLA), poly(D,L-lactide) (PLA), poly(glycolide) (PGA), poly(L-lactide-co-D,L-Lactide) (PLLA/PLA), poly(L-lactide-co-glycolide) (PLA/PGA), poly(glycolide-co-trimethylene carbonate) (PGA/PTMC), polydioxanone (PDS), polycaprolactone (PCL), polyhydroxybutyrate (PHBT), poly(phosphazenes), poly(D,L-lactide-co-caprolactone) (PLA/PCL), poly(glycolide-co-caprolactone) (PGA/PCL), poly(phosphase ester) and polyanhydrides. Other suitable materials, depending on a particular application, include hydrogels, gelatins, collagens, proteins, sodium alginate, karaya gum, guar gum, agar, algin, carrageenans, pectins, xanthan, starch based gums, hydroxyalkyl and ethyl ethers of cellulose, sodium carboxymethyl cellulose, polyvinyl alcohol, and hydrophilic polyurethanes.

For example, a synthetic sheet may be used to wrap around a MCS or AMCS to support bone growth. Alternately, synthetic scaffolding may be rods or bars or the like, which pass through in-line holes in the respective segments. Alternately, synthetic scaffolding may be in the form of a frame that surrounds or encompasses the bulk of each segment,
5 or the bulk of the demineralized segments, MCS, or AMCS that have flexible regions requiring structural support in the particular application in a patient in need thereof. This is employed, for instance, to add structural integrity to or around one or more segments, at least one of which has a high percentage of demineralized bone, or is otherwise in need of such additional structural support. Examples of synthetic scaffolding designs, which
10 are not meant to be limiting, are provided in Figure 31.

Another aspect of the invention is an assembled graft implant that is formed from at least three segments that interlock along abutting edges with one another. The shape of each segment is such that upon final assembly the major plane of each segment is non-coplanar in relation to the other segments, e.g., the segments do not lie parallel to one another. For example, Figure 32 shows a four-piece assembled graft implant, 3200, forming a roughly circular shape. This is made up of segments 3201, 3202, 3203, and 3204. Each segment has a male edge, 3205, and a female edge, 3206, which are designed to mate with an adjoining edge. One male edge slides into a female edge of an adjacent segment, and this process continues for other edges to complete a desired assembly.
15 When the joints of the edges interlock, as shown in Figure 32, the joints hold the segments together.

In a preferred embodiment, assembling three or more segments results in the formation of a central channel. A central channel, 3207, is shown in Figure 32. A central channel can be filled with osteogenic material, or may serve other purposes.
25

The interlocking edges are of shapes known by those skilled in the art to provide an interlocking joint. Examples, not meant to be limiting, of mateable joint designs (e.g.,
30 shapes where one part fits into or around the other) include ball and socket (as shown), tongue and groove, and mortise and tenon, such as a dovetail joint.

Also, where a portion of the body of the recipient has a need to remain intact (unsevered) yet there is a need to surround that portion with a structural support or to provide a protective barrier, segments of the present invention may be used, where the edges do not truly interlock, as defined above, but have sufficient tolerance to permit the direct insertion of the male edge into the female edge, at once along the edges, rather than sliding from one end. This facilitates the assembly around the portion in need of structural support or protection. Optionally, one or more bands of resilient material are wrapped around the assembled structure to increase rigidity, and/or other means known in the art can be used to increase the bonding at the interlocking junctions (synthetic adhesives, bone paste, screws).

Another interlocking embodiment is two arcuate shaped segments, each having two edges of opposing interlocking edges. The edges are interlocked to form a circular or truncated circular shape, preferably with a central channel within. When the arcuate shape is a semicircle, the assembled graft is a circular. Examples, not meant to be limiting, are shown in Figure 33, wherein segment **3300** is interlocked with segment **3310** thereby forming a channel **3320**. The two embodiments shown comprise different interlocking configurations **3330**.

Referring to Figure 34, another interlocking embodiment of an assembled allograft is shown as **3400**, whose final cross-sectional shape is a ‘tee-’ or ‘cross’. The embodiment comprises at two individual segments **3401** and **3402** that comprise a slot **3405** longitudinally defined thereon. Thus, the segments comprise a body portion **3406** and a slotted portion **3407**. When the segments are assembled they form a bone block by interlocking pieces **3401** and **3402** together. As shown, the assembled implant presents four fins, **3410a-d**, that radiate from a center point, **3403**. The preferred length of the assembled allograft, **3400**, is approximately 2.5 mm, and the preferred diameter may range from approximately 2.0 to 12.0 mm. This assembled allograft is used for various applications where bone blocks are used. Preferably, embodiment **3400** is used in conjunction with bone-tendon-bone grafts. When used in bone-tendon or bone-tendon

bone applications, preferably two separate flexible bands (natural or synthetic) are looped over the top of the embodiment 3400 wherein one band contacts fins 3410a and c, and the second band contacts fins 3410b and d. When the bone block 3400 is positioned into a channel, such as a bone tunnel formed in a patient, the two bands are compressed 5 against the fins 3410a-d and thereby secured into place. Alternatively, the ends of the fins can comprise teeth or are otherwise irregular to further prevent slippage of the bands.

The interlocking segments described above may be made of cortical bone, cancellous 10 bone, or a combination of cortical and cancellous bone. The segments may be of allograft or xenograft material, and preferably is treated to reduce antigenicity. In accordance with the requirements of the application, the interlocking segments are mineralized, demineralized, mixed-composition, synthetic, or a combination of these. Synthetic materials, such as those described above, may also be used in forming a 15 segment, and alternately, in contributing to the connection of the segments in addition to the interlocking edges.

Based on the present disclosure, those skilled in the art will further appreciate that the cortical bone pins disclosed herein may have features defined thereon for various 20 applications. For example, not meant to be limiting, the shafts may contain stops, such that other pieces of bone inserted thereon can only travel a certain distance down the shaft before encountering the stop. The shaft may also contain through holes, to permit insertion of cotter pins or the like. Furthermore, the cortical bone shaft may be demineralized, mineralized, or partially demineralized. In one specific embodiment, the 25 end of the cortical shaft contains a tapped cannulation a short distance into the longitudinal end of the shaft. In this way, a screw may be driven into the cannulation to retain elements inserted over the shaft in association with the shaft. To accommodate the screw, the screw end bearing the cannulation may be partially demineralized, such that upon insertion of the retention screw, the shaft end does not shatter, but expands to 30 accommodate the increasing diameter of the screw as it is driven into the shaft. Naturally, in certain applications, it may be desirable for the cortical pins to be

cannulated throughout the longitudinal length thereof. However, care should be taken that this does not unduly weaken the overall compressive or torsional strength of the assembled implant. This may be addressed by including pins that are not cannulated, along with pins that are cannulated. The cannulated pins may be used in combination 5 with sutures or the like, in order to hold an implant in a specific orientation, until fusion with adjacent bone has proceeded to a sufficient extent for the implant to become stable without the sutures.

It will be appreciated from the present disclosure that implants that have classically been 10 fabricated from metals may be fabricated by assembling bone pieces. In addition, a benefit of the assembled graft according to this invention is that the components of the assembled graft can be derived from various anatomical structures, thus circumventing limitations normally resulting from having to obtain a graft from a particular anatomical source of a particular donor. Not only can the components be sourced from different 15 anatomies, but also different donors may yield various components for assembly into a unitary implant. The end result is maximization of the gift of donation and the preservation of precious tissue resources. As noted above, being able to pool tissues from different sources depends, to some significant extent, on the ability to treat portions of tissue harvested from different anatomies or donors so as to prevent any contamination of 20 a recipient with pathological or antigenic agents. A further benefit of the present invention is that different implants with height or width limitations due to the anatomical structures from which the implant has been derived may be pinned together to form implants of essentially any desired dimensions. In this fashion, an inventory of building blocks in combination with the appropriate assembly pins, threaded or unthreaded, is 25 useful to provide implants of essentially any dimensions in the course of given surgical procedure. According to this embodiment of the invention, for example, a cervical Smith-Robinson (CSR) of any desired height may be produced by attaching two or more existing CSR implants together with cortical bone pins. This is accomplished preferably using two machined CSR's of known height such that when added together, the desired 30 overall height is achieved. The two CSR's are stacked and drill holes are machined through the CSR bodies, following which the cortical bone pins are press-fit through the

thus machined holes. Preferably, the diameter of the pins is slightly greater than the diameter of the drilled holes, such that a tight press-fit is achieved.

From the present disclosure, it will further be appreciated that implants according to this

5 invention may be assembled in the operating room by a surgeon, using pre-formed implant pieces, from a kit. It will further be appreciated that the assembled implant pieces may be adhered to each other using any of a number of biologically acceptable glues, pastes and the like. In one such embodiment, the assembled implant pieces are assembled using a polymethyl-methacrylate glue, a cyanoacrylate glue, or any other 10 adhesive known in the art, so long as the use of such an adhesive is confirmed to be non-toxic. It will further be appreciated that in forming the assembled grafts according to the present invention, it is acceptable, although not required, for interlocking features to be included on abutting faces of implant segments to be assembled together. Where such 15 features are included, it is preferred for the adjacent features to be complementary, such that a protrusion on a first surface is met by a compatible indentation in the abutting surface. Such abutting features assist to provide torsional and structural strength to the assembled implant, and to relieve a measure of stress on the cortical bone pins used to assemble the implant.

20 According to US patent 6,025,538, an elaborate system is disclosed for ensuring that a bore is provided in mating surfaces of a composite implant such that the bore is angularly aligned with respect to mating surfaces so as to be oblique to the plane of each mating surface. This is not required according to the present invention.

25 According to US patent 5,899,939, layers of bone are juxtaposed, but no mechanical fixation of the various layers to each other is provided for, such as the cortical bone pins disclosed herein.

Having generally described this invention, including the methods of manufacture and use 30 thereof, including the best mode thereof, those skilled in the art will appreciate that a large number of variations on the principles described herein may be accomplished.

Thus, the specifics of this description and the attached drawings should not be interpreted to limit the scope of this invention to the specifics thereof. Rather, the scope of this invention should be evaluated with reference to the claims appended hereto.

1 2 3 4 5 6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23 24 25 26 27 28 29 30 31 32 33 34 35 36 37 38 39 40 41 42 43 44 45 46 47 48 49 50 51 52 53 54 55 56 57 58 59 60 61 62 63 64 65 66 67 68 69 70 71 72 73 74 75 76 77 78 79 80 81 82 83 84 85 86 87 88 89 90 91 92 93 94 95 96 97 98 99 100